Acta Veterinaria (Beograd), Vol. 59, No. 2-3, 243-253, 2009.

DOI: 10.2298/AVB0903243

UDK 619:616-089.844

## HISTOLOGICAL AND IMMUNOHISTOCHEMICAL EVALUATIONS OF RAT SOFT TISSUE RESPONSE TO BIOCERAMICAL IMPLANTS

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### (Received 9. January 2009)

The purpose of this study was to evaluate the tissue response induced by bioceramical materials (BCM) implanted in rat subcutaneous tissue. Thirty two rats were assigned to 6 groups, as following: control group i.e. not treated; dental ceramic (DC) implants; alfa tricalcium phosphate synthetised at 22 MPa ( $\alpha$ TCP22) and at 45 MPa ( $\alpha$ TCP45); hydroxyapatite synthetised at 22 MPa (HAP22) and at 45 MPa (HAP45). Contra lateral sides of all test animals represented the blank control surgically incisied at the paravertebral sockets. The experimental groups received subcutaneous implants of the test BCM materials. Samples were collected after 14 days and processed histologically. Inflammatory reactions were noted microscopically. The inflammatory infiltrate consisted of lymphocytes, polimorphonuclears, macrophages and mastocytes. At same time there were signs of increased fibrosis around the graft places.

In conclusion, the implant sides compared with surgical incision wounds induced a foreign body-type granuloma with subsequent fibrosis around the grafts. The presence of a capsule at the interface with BCM in rat subcutis did not elicit any remarkable immune responses, thus being considered biocompatible. By evaluating different responses according to BCM, the most intense tissue reaction was noticed at HAP45, graded as severe, and mild to moderate for DC, HAP22 and alfa tricaltium phosphate.

Key words: bioceramics, biocompatibility, histology, subcutaneous tissue

## INTRODUCTION

Under physicochemical stimulations some signals will be generated at the cell level within the tissue and they regulate metabolic and biosynthetic activities.

The extracellular matrix makes the cell-matrix interactions which affect cell signalling in the tissue and the generating processes (Butler *et al.*, 2000).

Factors relating to the organization of the extracelular matrix macromolecules (e.g. various types of collagen and proteoglicans) (Hardingham and Fosang, 1992), and the heterogeneous cellular and compositional distributions within the tissue (Mow, 1998) play a significant role in defining the mechano-electrochemical environment around tissue cells. It is not known to which stimuli these cells are responding (e.g., fluid pressure or solid stress, viscous shear stress, osmotic pressure or hydrodynamic pressure).

From the bioengineering viewpoint, the lack of knowledge of cell-regulating signals is due, in part, to the difficulty of developing detailed and accurate constitutive laws for soft tissue and tissue cells (Tamai *et al.*, 2007).

Biomaterials used in all medical devices and implants can be classified under two categories, namely: 1. biological substitutes; 2. synthetic materials which include: a) metallic, b) polymeric, c) ceramic, d) composite materials). Each of these materials has it own characteristics (Janackovic *et al.*, 2003).

Ceramic materials, while very stabile and hard, suffer brittle fractures and cannot take on tensile forces (Sun and Leong, 2003). The tissue response to graft material is among other parameters, related to the characteristics of the material (Krsljak *et al.*, 2005).

This investigation brings an integrated approach to the host tissue response after a 2 week implantation period with the aim to evaluate specificities of soft tissue reactions on different types of bioceramic materials, and comparing them with subcutaneous responses following surgical incision.

### MATERIAL AND METHODS

## Materials

The tested BCM were obtained at the Faculty of Technology and Metallurgy, Belgrade University: dental ceramic (DC); alfa tricalcium phosphate synthesised at 22 MPa ( $\alpha$ TCP22); alfa tricalcium phosphate synthesised at 45 MPa ( $\alpha$ TCP45); hidroxyapatite synthesised at 22 MPa (HAP22); hidroxyapatite synthesised at 45 MPa (HAP45) (Figure 1).

Dental ceramic (DC) was obtained by the commercially made bioinert dental ceramics VITAVMK 95. The samples were prepared by mixing the ceramic powder with VITA modelling Fluid and shaped at 5x2 mm diameter. The samples were air heated at 600°C for 6 minutes, and after that heated up to 930° C with the heating rate of 55°C/min in vacuum. The cooled samples were after that glazed with Vita Akzent Powder mixed with Vita akzent Fluid, and heated at 600° C for 4 min.

The calcium phosphate materials were prepared chemically by synthesizing calcium-hydroxyapatite by the method of modified hydrothermal reaction of Ca(EDTA)<sup>2-</sup> in phosphate solutions. The impact of concentrations of Ca<sup>2+</sup> and PO<sub>4</sub><sup>3-</sup> - ions in the initial solution upon the morphology of synthesized HAP particles and attaining the  $\alpha$ -TCP phase after frying of obtained HAP powders was

investigated. These materials were obtained at pressures of 22 and 45 Mpa (Figure 1).



a) HAP1

a) HAP2

Figure 1. SEM particules of HAP powder obtained by hydrothermal method and dried at 105°C: a) HAP1, b) HAP2

As the starting supstrates for the synthesis of calcium-hydroxyapatite used were:

- calcium-nitrate tetrahydrate, Ca(NO<sub>3</sub>)<sub>2</sub> · 4H<sub>2</sub>O
- sodium salt of ethylenediamineted acetic acid (EDTA)
- sodium-phosphate dihydrate, NaH<sub>2</sub>PO<sub>4</sub>· 2H<sub>2</sub>O
- urea, p.a. purity.

# Animals and husbandry

Wistar-Albino rats (n=32) of both sex (average weights 250 gr) obtained from the Vivarium of the Institute of Physiology, School of Medicine Belgrade University, were randomly assigned to 2 groups, as follows: control, treated and 5 groups with subcutaneous implants.

The animals were anesthetized with aether. The surgical field was shaved and disinfected and two parallel paravertebral skin incisions were made. The subcutaneous tissue on the place of the right incision was prepared in the form of a pocket which was used for implantation of BCM. Both incisions were sutured and an antiseptic stick was applied.

## Histological studies and immunostaining

Two weeks after implantation the animals were measured and sacrificed by an overdose of aether. Tissue samples with implanted BCM, were fixed in 10% buffered formalin for 24 - 48 hours. After standard processing in an automated tissue processor, tissue samples were embedded in paraffin blocks. The 5  $\mu$ m thick paraffin sections were stained with haematoxylin and eosin (H&E) and toluidine blue (TB).

Immunohistologic investigation was performed with CD3 antibodies. After incubation primary antibodies (Polyclonal rabbit Antihuman CD3, DAKO, A0452,

and secondary biotinized antibodies (antimouse / antirabbit from comercial kit for IHC - ChemMate DAKO Citomation, Danmark, catalogue number K5003, bottle A) were used. For visualisation chromogen-DAB (3,3' diaminobenzidin) has been used which coloured brown the positive reaction site.

### Biocompatibility of medical devices

In this investigation ISO 10993 standards were used, specific to the testing and evaluation of local reactions to implanted materials. (*Upman et al.*,2004). The modification of ISO 10993-10:2002/ Amd 1: 2006 Biological evaluation of medical devices, Part 10: The test for irritation and delayed-type of hypersensitivity was also applied.

The grades for microscopical evaluations for all the animals in the test groups were calculated and the obtained sum divided by the number of observations to obtain a test group average for the irritant effects on soft tissues (Table 1).

Irritation index of soft tissue reaction to BCM	(IrI)					
Average grade	Description of response					
0	None					
1-5	Minimal					
6-10	Mild					
11-15	Moderate					
16-20	Marked					
	•					

Table 1. Irritation index of soft tissue reaction to BCM (Irl)

The study was conducted following the guidelines of the Belgrade School of Medicine.

### RESULTS

Scores of the evaluation of soft tissue response for Irritation index (Iri) were given as follows: absent (0), minimal (1), mild (2), moderate (3), and marked (4). (Table 2).

Inflammatory infiltrate and fibrosis intensity around the graft particles were analysed semi-quantitatively, under light microscopy attributing scores according to the level of inflammatory reactions (inflammatory infiltrate) and reparative processes (fibrosis, angioblastic and fibroblastic proliferation).

In the blank control group (contra lateral sides with surgical incisions), was possible to observe a granulation tissue rich in fibroblasts and blood capillaries, as well as large macrophages.

Deastian	Numerical grading										
Reaction		HI	DC	HI,	TCP22	HITC	P45	HI, H	AP22	HI, F	IAP45
EPITEL											
Normal, intact	0	1	1	1	1	1	1	1	1	1	1
Cell degeneration	1										
Metaplasia	2										
Focal erosion	3										
Generalized erosion	4										
LEUCOCYTE INFILTRATION (per high power fild)											
Absent	0										
Minimal (less than 25)	1	1		1		1		1		1	
Mild (26-50)	2		2		2				2		
Moderate (51-100)	3						3				
Marked (up to 100)	4										4
VASCULAR CONGESTION											
Absent	0										
Minimal	1	1		1		1		1		1	
Mild	2		2		2				2		
Moderate	3						3				
Marked, with disruption of vessels	4										4
OEDEMA											
Absent	0										
Minimal	1	1		1	1			1			
Mild	2		2			2				2	
Moderate	3						3				
Marked	4								4		4
CAPSULE											
Absent	0	0		0		0		0		0	
Minimal	1										
Mild / thin	2		2		2						
Moderate	3						3		3		
Marked / thick	4										4

## Table 2. Grading system for microscopic examination of soft tissue reaction

A fibrous capsule and an inflammatory reaction were present surrounding the implants. The inflammatory infiltrate consisted mostly of lymphocytes, macrophages and polimorphonuclears. The inflammatory reactions varied from mild to severe (Figure 2). The thickness varied from thinnest for DC and TCP22 evaluated as mild, moderate for TCP45 and HAP22, and marked, very thick for HAP45.

In all test samples at the contra lateral sides of the blank control a line of surgical incision from the epidermis to cutaneous muscle was noted, and was characterized with the presence of fibroblasts, fibrocytes, angioblasts and collagen fibers.

The subcutaneous connective tissue was mildly to moderately oedematous, containing macrophages, lymphocytes, eosinophils, and siderophages. These changes were graded from 1 (mild) to 4 (marked) according to BCM response differences.

Moderate fibroblastic and angioblastic proliferation and mild fibrosis were detected in the adjusting soft tissue. Small foci of macrophages containing phagocyted material were seen (Figure 3), the most remarkable in HAP45 specimen. In same test samples a marked presence of eosinophiles was observed.





Figure 2. (H&E, 10x). HAP45. The thick capsule with numerous infiltrate cell populations

Figure 3. (H&E, 100x). HAP45. Eosinophiles, macrophages, lymphocytes among collagenous fibers infiltrating the loose connective tissue of the capsule

In total immunohistological (IHC) evaluations of tissue response in all tested groups, comparing the contra lateral sides with surgical incision (SI) and graft implant response of tissue, mild CD3+ response in the epidermis, dermis, subcutis and cutaneous muscle was noted.

The test sides including BCM had various responses evaluated from mild to severe, mild in DC, moderate at HAP22, TCP22, TCP45, and marked at HAP45. The results are illustrated in Table 3., Table 4 and Figure 4.

Acta Veterinaria (Beograd), Vol. 59. No. 2-3, 243-253, 2009. Marković Danica *et al.*: Histological and immunohistochemical evaluations of rat soft tissue response to bioceramical implants



Figure 4. (IHC), CD3 positive staining in the soft tissue of tested animals. (A) SI on tested animals presented with concentrated CD3+ cells at the area of healing subepidermal soft tissue, 100x. (B) HAP45, the marked presence of CD3+ cells in deep subcutis surrounding the graft place, 100x. (C) DC, at adjacent graft implant soft tissue mild assigned CD3+ cells adjacent to hair follicle, 100x (D) TCP45, moderate presence of CD3+ cells in subcutis around the graft place, 10x





Table 4. Semi-quantitative evaluations of CD3+ cells IHC labelled in particular layers of soft tissue in tested animals grading lymphocite (CD3) presence in SI and BCM samples



#### DISCUSSION

Disruption of structural and functional integrity of the skin, caused by different factors, induces an overlapping pattern of events including haemostasis, inflammation and epithelization, as well as formation of granulation tissue and tissue remodelling (Todorovic *et al.*, 2008). Few hours after injury the wound site is invaded with inflammatory cells: neutrophils, first, than monocytes, macrophages, fibroblasts and lymphocytes (Diegelman *et al.*, 2004). After 3 days the collagen fibrils can be seen in the linear incision of the skin (Werner *et al.*, 2003). Many of the growth factors and cytokines are released at that time. As the proliferative phase progresses, the predominant cells in the wound site are reparatory cells producing the new matrix needed for structure and function repair of the injured tissue (Whitney, 2005).

In the presence of graft implants of BCM materials due to foreign bodytissue reaction, and moreover, specific biocompatible or noncompatible response of host tissue develops (Bernath and Szabo, 2003). A variety of artificial materials has been used to fill in bone defects. Ideally, bone grafts should be biocompatible, causing minimal fibrotic reactions. They should undergo remodelling and support new bone formation. Generally, bioactive ceramics have the ability to bond directly to bone tissue, and have both osteointegrative and osteoinductive properties, at the same tame having improved mechanical properties over other bone substitutes (Danilovic *et al.*, 2007).

In the search for ideal biocompatible materials many different methods have been described for assessing tissue toxicity (Spangberg, 1988.) *In vivo* experimental models must be used to obtain answers to local tissue response to bioceramical implants (Pissiotis and Spangberg, 2000; Ozbes *et al.*, 2003; Saidon *et al.*, 2003). The majority of studies have been performed on soft tissue (Stojanovic *et al.*, 2008). Spangberg (1990) commented that such implantation was easy to do and required minor surgical skills. The observation period after inserting implants must be established in such a way that both short-term reactions, as well as long-term healing can be observed. It is important to obtain information about the initial effect of bio ceramic materials on tissue. Surgical implantation introduces such tissue trauma and subsequent surgical inflammation that it becomes practically impossible to distinguish the tissue response from that created by the material being investigated (Spangberg, 1990).

The implanted materials led to moderate or severe inflammatory responses initially, but the response decreased in time with an increasingly thickening fibrous connective tissue capsule forming around the grafts. This response is moderate at the beginning and it is decreasing in magnitude with time. This form of reaction is in agreement with the Dental Association technical requisites (ANSI/ADA, 1982) in determining a material as biologically acceptable.

### CONCLUSION

The examined tissue samples showed mild inflammatory tissue reactions, primarily due to surgical trauma.

The most reactive tissue was under the influence of HAP45 implants, where in the tissue surrounding the graft lymphocytes, macrophages, siderophages, plasmocytes, mastocytes and eosinophiles were observed. In same cases the widest capsule was presented with swelling surrounding tissue.

The test material comparing with surgical incision wounds induced a foreign body – type granuloma with subsequent fibrosis around the graft implants, presence of capsule at interface with BCM in rat subcutaneous tissue and did not elicit any remarkable immune response, thus upon evaluation are considered biocompatible.

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## HISTOLOŠKA I IMUNOHISTOHEMIJSKA PROCENA REAKCIJE MEKOG TKIVA PACOVA NA BIOKERAMIČKE IMPLANTE

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## SADRŽAJ

Svrha ove studije je bila procena tkivnog odgovora indukovanog biokeramičkim materijalima (BCM) inplantiranim u subkutano tkivo pacova. Trideset dva pacova je bilo podeljeno u sledećih 6 grupa: kontrolna grupa-neoperisana; inplantirane sa: dentalnom keramikom (DC); alfa trikalcijum fosfatima sintetisanim na 22 MPa ( $\alpha$ TCP22) i na 45 MPa ( $\alpha$ TCP45); hidroksiapatitom sintetisanim na 22 MPa (HAP22) i na 45 MPa ( $\alpha$ TCP45). Kontralateralne strane svih životinja bile su slepa kontrola i urađene su kao džepovi hirurške incizije u subkutanom tkivu. Eksperimentalne grupe su imale subkutano inplantirane biokeramičke materijale. Uzorci su sakupljeni posle 14 dana i sprovedeni u histološkoj proceduri, a inflamatorna reakcija je praćena mikroskopski. Inflamatorni infiltrat se sastojao od limfocita, polimorfonuklearnih leukocita, makrofaga i mastocita. Istovremeno su uočeni znaci rastuće fibroze oko mesta graftova.

Inplantirana mesta u poređenju sa hirurškim ranama indukuju granulom karakterističnog tipa na strano telo sa posledičnom fibrozom oko graftova, kapsulom na dodirnoj površini sa BCM u subkutisu pacova, ne izazivajući uočljivu imunološku reakciju, tako da odgovor tkiva ukazuje na biokompatibilnost. Procenjivanjem odgovora sa različitim BCM, zabeležena je najintenzivnija (snažna) tkivna reakcija kod HAP45 inplanta, a blaga do umerena kod DC, HAP22 i alfa trikalcijumfosfata.